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ADVANCEMENTS AND CHALLENGES IN SIMULATION DESIGNS FOR LATERAL FLOW ASSAY BIOSENSORS IN INFECTIOUS DISEASE DIAGNOSTICS

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Abstract

Biosensors for Lateral Flow Assay (LFA) have emerged as essential instruments for the quick and on-site diagnosis of infectious diseases. To improve the sensitivity, specificity, and adaptability of LFAs, this study examines the various simulation designs used in their creation and optimization. These simulations integrate cutting-edge computational methods, such as AI-driven algorithms and high-performance computing, to offer vital insights into the intricate biological interactions and environmental variables affecting LFA performance. The integration of real-time data, the creation of customized and accurate diagnostics, and the focus on ecologically friendly and sustainable design techniques are important future directions. Nevertheless, the field faces many difficulties, including reproducibility and scalability of simulation models, integration of diverse datasets, and accurate modeling of biological complexity. To meet the demands of new infectious disease threats, LFA biosensors must continue to evolve, which will require addressing these issues. This review addresses the challenges that need to be solved to fully utilize these important diagnostic tools, as well as the state of LFA simulation designs today and future developments.

Keywords: Lateral flow assay, Simulation, Biosensor, Infectious disease

1.0 Introduction

Lateral Flow Assay (LFA) biosensors have become pivotal in the diagnosis of infectious diseases, offering a rapid, user-friendly, and cost-effective solution for point-of-care testing (1). These devices are particularly valuable in settings where laboratory infrastructure is limited, such as in remote regions or during public health emergencies. The design and optimization of LFAs pose significant challenges despite their widespread adoption, particularly in achieving high sensitivity, specificity, and reliability all of which are essential for accurate disease detection (2). Researchers are using more sophisticated simulation techniques to address these issues, which has changed the way LFA designs are created. The intricate relationships that exist within an LFA can be modeled and

optimized in a virtual environment that is made possible by simulation designs. Through these simulations, scientists can forecast the behavior of various assay components, including membrane materials, antibodies, and nanoparticle labels, under various scenarios. Researchers can shorten the time and expense of development by improving the assay's sensitivity and specificity in a virtual environment before proceeding to the experimental stage (3). This strategy is especially crucial when it comes to infectious diseases, as controlling outbreaks requires the quick development of accurate diagnostics. The role that LFAs played in the COVID-19 pandemic highlights the importance of these biomarkers in the diagnosis of infectious diseases (4). The combination of CRISPR/Cas9 with recombinase polymerase amplification (RPA) in LFAs significantly improves sensitivity by eliminating primer-dimer interference, allowing detection of *Staphylococcus aureus* at low concentrations (63 CFU/mL) (5). Recent advancements in nanomaterials, such as gold and silver nanoparticles, enhance signal generation, improving the sensitivity and specificity of LFAs (6). LFAs are designed for ease of use, making them suitable for resource-limited settings, which is critical in combating infectious diseases globally (7). The simplicity of LFAs allows for immediate results, facilitating timely medical interventions during pandemics (8). LFAs played a crucial role in mass testing initiatives, facilitating extensive screening and assisting in reducing the virus's spread. The use of simulation techniques sped up the development of these assays by enabling quick iteration and assay design optimization. The best designs were chosen by using simulations to forecast how LFAs would behave in various sample conditions and environmental factors. Nevertheless, there are certain difficulties with using simulation in LFA design. The biological interactions that take place within an LFA are difficult to accurately model, necessitating advanced algorithms and high-performance computer resources(9). Because biological systems are naturally unpredictable, assay performance can be impacted by a variety of factors, including sample matrix effects, protein binding affinities, and environmental factors. To handle these complexities, advanced computational techniques such as machine learning and high-performance computing are being used more and more; however, there are still major obstacles in the way of creating models that are both computationally efficient and accurate.

As the field of diagnostics moves towards personalized and precision medicine, there is a growing demand for LFAs that can be tailored to individual patient profiles (10). This shift presents new challenges for simulation design, as models must now account for the detection of unique biomarkers or multiple targets within a single assay. Moreover, the integration of real-time data into simulation models is becoming increasingly important, allowing for the dynamic adaptation of LFAs in response to emerging infectious diseases. Practical issues like the development of sustainable materials and the scalability of simulation designs for large-scale manufacturing must be considered in addition to these technical difficulties. The role of simulation in LFA development is expected to become even more crucial as the need for quick and accurate diagnostic tools increases globally, especially in response to new infectious threats. This work examines the various simulation designs that have been employed in the creation of LFA biosensors for infectious diseases, emphasizing the developments in computational methods, the difficulties associated with simulating LFA performance, and the prospects for the field going forward. The purpose of this study is to shed light on additional ways to use these instruments to enhance the functionality and appearance of these essential diagnostic tools.

2.0 Modeling Lateral Flow Mechanisms:

Developing effective diagnostic tools for infectious diseases requires understanding and modeling lateral flow mechanisms. Lateral flow immunoassays (LFIA) have become a popular choice for point-of-care testing, especially in areas with limited resources (11). A 3D model utilizing the Richards equation and numerical simulations illustrates the impact of flow dynamics on LFIA performance. Factors like the amount of reporter particles and the speed of reactions have a big impact on how well both sandwich and competitive LFIA tests can detect substances (12). Urine is a perfect source of biomarkers because it can be easily collected non-invasively and reflects general changes in the body. Urinary biomarkers in LFAs can help speed up the diagnosis of infectious diseases, leading to better patient outcomes and decreased antibiotic use (13). The potential of lateral flow tests (LFTs) for decentralized testing was brought to the forefront by the COVID-19 pandemic. Advancements in bioengineering are crucial for improving the accuracy and precision of LFTs, which play a crucial role in controlling infectious disease outbreaks (14). Sophisticated mathematical models, such as stochastic and differential equations, offer understanding of how infectious diseases spread. These models have the potential to shape public health strategies and improve responses to outbreaks.

3.0. Parameter Optimization

3.1 Flow Dynamics

Lateral flow assays (LFAs) are now essential for quick diagnosis of infectious diseases due to their simplicity and cost-effectiveness. The performance of LFAs depends on the flow dynamics, which impact the sensitivity and speed of results. LFAs use capillary action to pull samples through a porous membrane, which helps the sample interact with immobilized reagents necessary for pathogen detection (15). The structure consists of a sample pad, conjugate pad, and test line, with flow dynamics that are fine-tuned to guarantee swift and effective bonding of antigens or antibodies, essential for prompt detection (16). Recent developments are centered on incorporating nanotechnology to enhance the sensitivity of LFAs, enabling the identification of low levels of biomarkers, which is especially advantageous in areas with limited resources (17). Results from the simulation showed that changing the composition of the membrane and the materials of the conjugate pad had a significant impact on the lateral flow dynamics. Improved designs showed better analyte movement and superior binding rates, leading to quicker and more precise outcomes.

3.2 Parameter Sensitivity Analysis

Sensitivity analyses emphasized the significance of certain parameters in LFA efficiency. For example, changing the number of capture molecules on the test line or altering the wicking material affected the limit of detection and reduced false positives. Parameter sensitivity analysis in lateral flow assay (LFA) biosensors for infectious diseases aims to improve sensitivity and detection limits by optimizing different design components. Recent research emphasizes various creative methods to accomplish this objective. The implementation of laser-micromachined microchannels on nitrocellulose membranes greatly enhanced immunological response rates by 950%, resulting in a 40% boost in signal sensitivity as compared to conventional LFAs (15). A polydopamine@MnO₂ nanocomposite-enhanced peptide-based LFA exhibited superior performance compared to traditional methods, with a detection limit of 8.01 pg/mL for SARS-CoV-2, surpassing them by 18.7 times. This amplification method combines both natural melanin and nanozyme catalytic enhancement (16). By

regulating sample flow and increasing reaction times, mechanically compressed barriers within cellulose membrane LFAs enhanced sensitivity from 2.0 nM to 0.5 nM without the need for extra materials (17). These developments demonstrate the important function of parameter sensitivity analysis in creating efficient LFAs for quick infectious disease testing. Despite this, there are still difficulties in finding the right balance between sensitivity, cost-effectiveness, and user-friendliness, especially in places with limited resources (18).

4.0 Discussion

LFAs have played a crucial role in diagnosing infectious diseases by providing fast, easy-to-use, and economical testing options. Yet, the complexity of designing and optimizing these biosensors is inherent, necessitating a profound comprehension of the biological, chemical, and physical interactions involved in the assay. Simulation designs have become impactful instruments in this scenario, enabling researchers to forecast and enhance the performance of LFAs prior to transitioning to the experimental stage. Recent improvements in computational methods have greatly improved the functionality of simulation models. HPC has made it possible to simulate increasingly intricate systems more quickly, thus facilitating the analysis of numerous variables and interactions at the same time. Machine learning algorithms, especially those using deep learning, have enhanced these simulations by uncovering patterns and connections that traditional methods may not easily detect. Algorithms can optimize antibody selection, forecast sample flow dynamics in the assay, and assess how environmental factors affect assay performance. LFAs are advantageous for use in areas with limited resources, particularly during pandemics, due to their rapid results (19). The affordable manufacturing costs of LFAs make them suitable for use in developing countries (20). The utilization of nanomaterials like gold nanoparticles and green nanomaterials has increased sensitivity and specificity, improving the overall efficiency of LFAs (21). LFAs can efficiently make use of urinary biomarkers to diagnose infectious diseases, providing a non-invasive and readily available testing approach (22). The latest developments involve combining CRISPR/Cas9 with LFAs, which increases sensitivity and minimizes interference from primer-dimer formations, ultimately enhancing diagnostic precision for pathogens such as *Staphylococcus aureus* (19). The incorporation of these sophisticated computational technologies has enabled more precise forecasting of LFAs' real-world performance. This is especially crucial when dealing with infectious diseases, as differences in samples and environmental conditions can have a major impact on the accuracy of diagnostics. By mimicking these elements, scientists can create tests that are stronger and more trustworthy, decreasing the chance of inaccurate results. Additionally, simulations can speed up the development process by enabling quick iteration and testing of various designs.

5.0 Conclusion

Exploring different simulation designs for Lateral Flow Assay (LFA) biosensors shows potential in improving the diagnostic abilities of these commonly-used tools for identifying infectious diseases. This review emphasizes the importance of simulation models in improving the performance, sensitivity, and specificity of LFAs, crucial for precise and prompt diagnosis, particularly in settings with limited resources. Simulation models have played a key role in overcoming the typical constraints of LFAs by enhancing their sensitivity and specificity. Through manipulating design factors like sample flow rate, antibody binding kinetics, and nitrocellulose membrane properties, researchers have forecasted and enhanced the assay's efficiency prior to prototyping. This proactive method greatly decreases the need for trial and error during the design phase, resulting in improved diagnostic

accuracy and efficiency. The successful modeling of advanced materials like nanoparticles and engineered proteins in LFA designs has been achieved through simulations. These simulations offer understanding into how these materials behave in different situations, which helps in improving the features of future LFAs. An example is how gold nanoparticles have been proven to enhance visual detection limits, and simulations have been useful in optimizing the size and concentration of these particles for maximum signal output. The adaptability of LFA biosensors, when paired with simulation capabilities, has been crucial in quickly adjusting these tests for identifying new infectious diseases. Simulation models enable rapid reconfiguration of assay components to target new pathogens, making LFAs a valuable tool in tackling global outbreaks like COVID-19, Zika virus, and more. The capacity to mimic how new antigens interacts with current detection components speeds up the development process and guarantees that LFAs can be quickly implemented in reaction to public needs.

6.0 Future Directions & Challenges

As the field of lateral flow assay (LFA) biosensors continues to advance, the use of simulation designs in their development is becoming increasingly sophisticated. As simulation models become more complex, the need for enhanced computational power grows. High-Performance Computing (HPC) systems and cloud-based computing resources will be increasingly utilized to run large-scale simulations that incorporate multiple variables and detailed biological interactions. This will allow for more precise and faster simulations, facilitating the rapid development of highly optimized LFAs (23). Future LFA simulations will increasingly integrate real-time data inputs, allowing for adaptive assay design that can respond dynamically to emerging infectious disease threats. By incorporating AI, these simulations can continuously update and refine the LFA design based on real-time epidemiological data, ensuring that the assays remain relevant and effective. AI and machine learning will play a significant role in predictive modeling, where simulations can forecast the performance of LFAs in new or changing environments. This will be particularly important in developing assays for emerging pathogens, where historical data may be limited (24). The future of LFAs lies in their ability to be tailored to individual patient profiles, particularly in the context of personalized medicine. Simulations will be crucial in designing assays that detect biomarkers unique to specific patients, thereby enabling more accurate diagnostics and targeted therapies (25). Precision diagnostics will require simulations that can model the behavior of LFAs in highly specific conditions, such as detecting low-abundance biomarkers or distinguishing between closely related pathogens. This will push the boundaries of current simulation techniques and require significant advancements in both software and hardware (26). Future simulations will focus on the environmental impact of LFA biosensors, modeling the use of sustainable materials and green manufacturing processes (27). This will include the development of biodegradable components and the reduction of harmful byproducts during production. Simulations will help in designing LFAs that are both effective and environmentally responsible. Accurately representing the intricate biological interactions that take place in LFAs is a key challenge in simulation design. Biological systems are complex by nature, involving many factors like protein binding affinities, fluid dynamics, and sample variability. Creating a simulation that accurately represents this complexity necessitates intricate models that are challenging to validate and require significant computational resources. Another obstacle is to guarantee the accuracy and reliability of these models. Minor inaccuracies in the simulation parameters may cause substantial discrepancies in the projected efficiency of the LFA, potentially leading to inadequate diagnostic outcomes. Validating these simulations against experimental data is crucial and can be a lengthy and expensive process to ensure accuracy.

Simulations for designing LFAs, particularly for new infectious diseases, frequently face challenges due to a lack of data. Limited availability of comprehensive data on emerging pathogens can hinder accurate modeling of their interaction with assay components. This restriction can impede the quick progress of efficient LFAs in the initial phase of an outbreak. Incorporating various datasets into one simulation model is also a major hurdle. LFAs need to consider the different types of data needed for variations in sample types, environmental conditions, and user handling. Merging these datasets to create a unified model that accurately mirrors real-life conditions is a challenging process that necessitates sophisticated data integration techniques. Scaling simulation models for commercial-level production of LFAs presents another challenge. While simulations may be effective for smaller designs, incorporating them to factor in larger manufacturing processes presents new challenges and factors to consider. It is crucial for LFAs to scale effectively while maintaining accuracy to enable their widespread deployment.

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8.0 Conflicts Of Interest

The Authors have no conflicts of interest in this work.

9.0 Ethical Approvals

The study does not involve experiments on animals or human subjects.

10.0 Data availability statement

There is no data for this review.

11.0 Informed consent

None.

12.0 References

1. Soh JH, Chan HM, Ying JY. Strategies for developing sensitive and specific nanoparticle-based lateral flow assays as point-of-care diagnostic device. *Nano Today* [Internet]. 2020 Feb [cited 2024 Aug 23];30:100831. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S1748013219305420>
2. Dey MK, Iftesum M, Devireddy R, Gartia MR. New technologies and reagents in lateral flow assay (LFA) designs for enhancing accuracy and sensitivity. *Anal Methods* [Internet]. 2023 [cited 2024 Aug 23];15(35):4351–76. Available from: <https://xlink.rsc.org/?DOI=D3AY00844D>
3. Ekert JE, Deakyne J, Pribul-Allen P, Terry R, Schofield C, Jeong CG, et al. Recommended Guidelines for Developing, Qualifying, and Implementing Complex In Vitro Models (CIVMs) for Drug Discovery. *SLAS Discovery* [Internet]. 2020 Dec [cited 2024 Aug 23];25(10):1174–90. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S2472555222066412>

4. Zhou Y, Wu Y, Ding L, Huang X, Xiong Y. Point-of-care COVID-19 diagnostics powered by lateral flow assay. *TrAC Trends in Analytical Chemistry* [Internet]. 2021 Dec [cited 2024 Aug 23];145:116452. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S0165993621002752>
5. Wang H, Wu Q, Yan C, Xu J, Qin X, Wang J, et al. CRISPR/Cas9 bridged recombinase polymerase amplification with lateral flow biosensor removing potential primer-dimer interference for robust *Staphylococcus aureus* assay. *Sensors and Actuators B: Chemical* [Internet]. 2022 Oct [cited 2024 Aug 23];369:132293. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S0925400522009352>
6. Wang Z, Zhao J, Xu X, Guo L, Xu L, Sun M, et al. An Overview for the Nanoparticles-Based Quantitative Lateral Flow Assay. *Small Methods* [Internet]. 2022 Jan [cited 2024 Aug 23];6(1):2101143. Available from: <https://onlinelibrary.wiley.com/doi/10.1002/smtd.202101143>
7. Shi X, Wang Z. The current advances and future perspectives of lateral flow immunoassay for infectious diseases. *Reviews in Medical Microbiology* [Internet]. 2021 Jul [cited 2024 Aug 23];32(3):183–9. Available from: <https://journals.lww.com/10.1097/MRM.0000000000000253>
8. Jiang N, Ahmed R, Damayantharan M, Ünal B, Butt H, Yetisen AK. Lateral and Vertical Flow Assays for Point-of-Care Diagnostics. *Adv Healthcare Materials* [Internet]. 2019 Jul [cited 2024 Aug 23];8(14):1900244. Available from: <https://onlinelibrary.wiley.com/doi/10.1002/adhm.201900244>
9. O’Sullivan S, Ali Z, Jiang X, Abdolvand R, Ünlü MS, Plácido Da Silva H, et al. Developments in Transduction, Connectivity and AI/Machine Learning for Point-of-Care Testing. *Sensors* [Internet]. 2019 Apr 23 [cited 2024 Aug 23];19(8):1917. Available from: <https://www.mdpi.com/1424-8220/19/8/1917>
10. Calabretta MM, Zangheri M, Lopreside A, Marchegiani E, Montali L, Simoni P, et al. Precision medicine, bioanalytics and nanomaterials: toward a new generation of personalized portable diagnostics. *Analyst* [Internet]. 2020 [cited 2024 Aug 23];145(8):2841–53. Available from: <https://xlink.rsc.org/?DOI=C9AN02041A>
11. Zhao X, Zhang Y, Niu Q, Wang L, Xing C, Wang Q, et al. Research on the Flow Characteristics and Reaction Mechanisms of Lateral Flow Immunoassay under Non-Uniform Flow. *Sensors* [Internet]. 2024 Mar 20 [cited 2024 Aug 23];24(6):1989. Available from: <https://www.mdpi.com/1424-8220/24/6/1989>
12. Patil AA, Kaushik P, Jain RD, Dandekar PP. Assessment of Urinary Biomarkers for Infectious Diseases Using Lateral Flow Assays: A Comprehensive Overview. *ACS Infect Dis* [Internet]. 2023 Jan 13 [cited 2024 Aug 23];9(1):9–22. Available from: <https://pubs.acs.org/doi/10.1021/acsinfecdis.2c00449>
13. Budd J, Miller BS, Weckman NE, Cherkaoui D, Huang D, Decruz AT, et al. Lateral flow test engineering and lessons learned from COVID-19. *Nat Rev Bioeng* [Internet]. 2023 Jan 19 [cited 2024 Aug 23];1(1):13–31. Available from: <https://www.nature.com/articles/s44222-022-00007-3>

14. Udriste C, Tevy I, Rasheed AS. Flow, Wind, and Stochastic Connectivity Modeling Infectious Diseases. Farza M, editor. Complexity [Internet]. 2021 Jan [cited 2024 Aug 23];2021(1):6395410. Available from: <https://onlinelibrary.wiley.com/doi/10.1155/2021/6395410>
15. Khatmi G, Klinavičius T, Simanavičius M, Silimavičius L, Tamulevičienė A, Rimkutė A, et al. Lateral Flow Assay Sensitivity and Signal Enhancement via Laser μ -Machined Constrains in Nitrocellulose Membrane [Internet]. 2024 [cited 2024 Aug 23]. Available from: <http://biorxiv.org/lookup/doi/10.1101/2024.05.09.593095>
16. Dong T, Zhang X, Yuan J, Lin Z, Yin P, Yu H, et al. Sensitive Lateral Flow Immunoassay Based on Specific Peptide and Superior Oxidase Mimics with a Universal Dual-Mode Significant Signal Amplification. Anal Chem [Internet]. 2023 Aug 22 [cited 2024 Aug 23];95(33):12532–40. Available from: <https://pubs.acs.org/doi/10.1021/acs.analchem.3c02821>
17. Vealan K, Joseph N, Alimat S, Karumbati AS, Thilakavathy K. Lateral flow assay: a promising rapid point-of-care testing tool for infections and non-communicable diseases. Asian Biomedicine [Internet]. 2023 Dec 1 [cited 2024 Aug 23];17(6):250–66. Available from: <https://www.sciendo.com/article/10.2478/abm-2023-0068>
18. Wu J, Dhingra R, Gambhir M, Remais JV. Sensitivity analysis of infectious disease models: methods, advances and their application. J R Soc Interface [Internet]. 2013 Sep 6 [cited 2024 Aug 23];10(86):20121018. Available from: <https://royalsocietypublishing.org/doi/10.1098/rsif.2012.1018>
19. Sohrabi H, Majidi MR, Fakhraei M, Jahanban-Esfahlan A, Hejazi M, Oroojalian F, et al. Lateral flow assays (LFA) for detection of pathogenic bacteria: A small point-of-care platform for diagnosis of human infectious diseases. Talanta [Internet]. 2022 Jun [cited 2024 Aug 23];243:123330. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S0039914022001266>
20. Rypar T, Bezdekova J, Pavelicova K, Vodova M, Adam V, Vaculovicova M, et al. Low-tech vs. high-tech approaches in μ PADs as a result of contrasting needs and capabilities of developed and developing countries focusing on diagnostics and point-of-care testing. Talanta [Internet]. 2024 Jan [cited 2024 Aug 23];266:124911. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S0039914023006628>
21. Sadeghi P, Sohrabi H, Hejazi M, Jahanban-Esfahlan A, Baradaran B, Tohidast M, et al. Lateral flow assays (LFA) as an alternative medical diagnosis method for detection of virus species: The intertwine of nanotechnology with sensing strategies. TrAC Trends in Analytical Chemistry [Internet]. 2021 Dec [cited 2024 Aug 23];145:116460. Available from: <https://linkinghub.elsevier.com/retrieve/pii/S0165993621002831>
22. Ates HC, Brunauer A, Von Stetten F, Urban GA, Güder F, Merkoçi A, et al. Integrated Devices for Non-Invasive Diagnostics. Adv Funct Materials [Internet]. 2021 Apr [cited 2024 Aug 23];31(15):2010388. Available from: <https://onlinelibrary.wiley.com/doi/10.1002/adfm.202010388>

23. Banegas-Luna AJ, Imbernón B, Llanes Castro A, Pérez-Garrido A, Cerón-Carrasco JP, Gesing S, et al. Advances in distributed computing with modern drug discovery. *Expert Opinion on Drug Discovery* [Internet]. 2019 Jan 2 [cited 2024 Aug 23];14(1):9–22. Available from: <https://www.tandfonline.com/doi/full/10.1080/17460441.2019.1552936>
24. Gaur K, Jagtap MM. Role of Artificial Intelligence and Machine Learning in Prediction, Diagnosis, and Prognosis of Cancer. *Cureus*. 2022 Nov;14(11):e31008.
25. Johnson KB, Wei WQ, Weeraratne D, Frisse ME, Misulis K, Rhee K, et al. Precision Medicine, AI, and the Future of Personalized Health Care. *Clin Transl Sci*. 2021 Jan;14(1):86–93.
26. Gradisteanu Pircalabioru G, Raileanu M, Dionisie MV, Lixandru-Petre IO, Iliescu C. Fast detection of bacterial gut pathogens on miniaturized devices: an overview. *Expert Review of Molecular Diagnostics* [Internet]. 2024 Mar 3 [cited 2024 Aug 23];24(3):201–18. Available from: <https://www.tandfonline.com/doi/full/10.1080/14737159.2024.2316756>
27. Ongaro AE, Ndlovu Z, Sollier E, Otieno C, Ondo P, Street A, et al. Engineering a sustainable future for point-of-care diagnostics and single-use microfluidic devices. *Lab Chip* [Internet]. 2022 [cited 2024 Aug 23];22(17):3122–37. Available from: <https://xlink.rsc.org/?DOI=D2LC00380E>